

#790 Separating the neural contributions to fMRI signal through Neural Prior Recovery.

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Background

- Standard confound correction consists of modeling and regressing confounds, but, it is unclear whether it can account for confounds while preserving neural activity (Power et al. (2020). Cereb Cortex).
 Alternative solution: isolate pre-defined neural sources (i.e. neural priors) from all other sources
 Sub-goal 1, reliability: Model scan-specific fMRI confounds in all forms (spatial and temporal)
- Sub-goal 2, specificity: maximize the relationship of recovered to neural activity
- Sub-goal 3, generalizability: automated framework with robust performance across datasets

Dataset and processing software

- Multi-site dataset: representative survey of data quality issues; 17 sites (5 not included); N=15 scans per site (Grandjean et al. (2020). NeuroImage.)
- Simultaneous mesoscale calcium imaging and fMRI: 10 subjects, 3 session X 9 runs per subject; with excitatory cell calcium marker (SLC)
- Processing: RABIES (<u>https://github.com/CoBrALab/RABIES</u>)

Algorithm Development

A)	Complementary PCA (C-PCA)		B)	B Neural Prior Recovery (NPR)		
Linear re	ear regression #1: fit timecourses Linear regression #2: fit spatial maps		C-PCA #1: derive scan-specific C-PCA #2: Recover neural priors		Confounds	A REAL PROPERTY OF THE REAL PROPERTY AND ADDRESS OF THE REAL PROPERTY AND ADDRESS OF THE REAL PROPERTY AND ADDRESS OF THE REAL PROPERTY ADDRESS OF THE REAL PROPE
	Target timeseries (X)	Target timeseries (X)	<u>non-</u>	Dirior (i.e. confound) sources while correcting non-prior sources Target timeseries (X) Target timeseries (X)	Dual regression	







Result 2: maximize relationship to calcium tracer



Figure 2: Impact of confounds on connectivity analyses, tested across 12 mouse fMRI acquisition sites. The top plot displays the distribution of correlations between the scan-level fits and prior network maps. The bottom plot shows the mean temporal correlation between the network timecourse and a set of confound component timecourses measured through dual regression (using group-ICA confound components described in Desrosiers-Gregoire et al. (2022. bioRxiv.); see example in **figure 1C**). Nuisance regression was varied (3 different columns) to include the regression of 6 motion parameters + WM/CSF signal, 6 motion parameters + global signal, or no regression.

Figure 3: A) Using simultaneous calcium and fMRI imaging (figure adapted from Lake et al. 2020), B) a prior of the somatomotor network was identified through group ICA in each modality independently (displayed on 2D cortical surface). A network timecourse is derived in each modality, and the two timecourses are then correlated after hemodynamic response function convolution of the calcium timecourse (gamma variate function: time to peak = 2.6 s, width = 1.2 s). fMRI confound correction consisted of scrubbing + highpass 0.01Hz + motion/WM/CSF regression.

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Implications

- We offer a generalizable framework for carrying automated confound correction while preserving neural activity. Can be carried out similarly in human studies.
- **Trade-off:** constrained to the set of priors, discard residuals. But in most studies, residuals are unknown (i.e. without validated neural origin).
- Open source code implemented in RABIES https://github.com/CoBrALab/RABIES